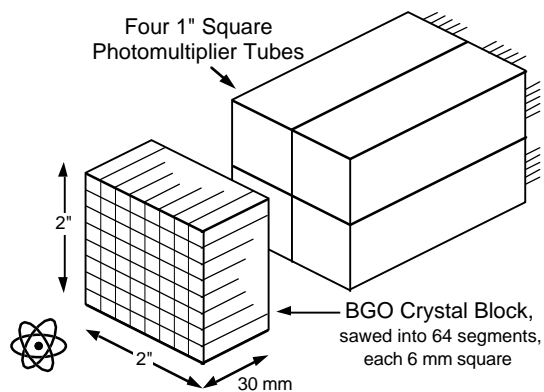


Application of New Detector Technology to PET

W.W. Moses
Lawrence Berkeley Laboratory

- Basic PET Detector Requirements
- New Photodetector Technologies
- PET Detector Modules based on
New Photodetectors
- Possible Scintillator Improvements

Conventional Block Detector Design



\$600 / in²
\$400 BGO
\$200 PMT

Hit crystal identified by Anger Logic

- 6 mm square crystals → 5 mm spatial resolution
- Detector block is 2 x 2 inches → 1.2 μ s in₂ dead time

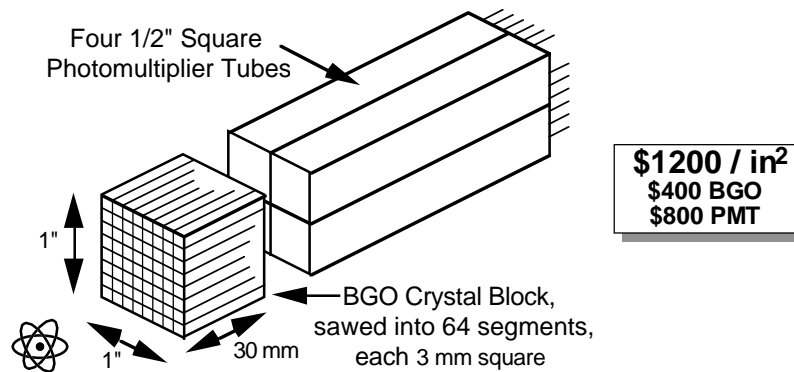
PET Detector Requirements

- Detect 511 keV Photons with
- <5 mm spatial resolution
 - <10 ns timing resolution
 - <100 keV energy resolution
 - “low” dead time (<1 μ s in)
 - “low” cost (<\$600 / in²)

2

2

“Shrunk” Conventional Block Detector

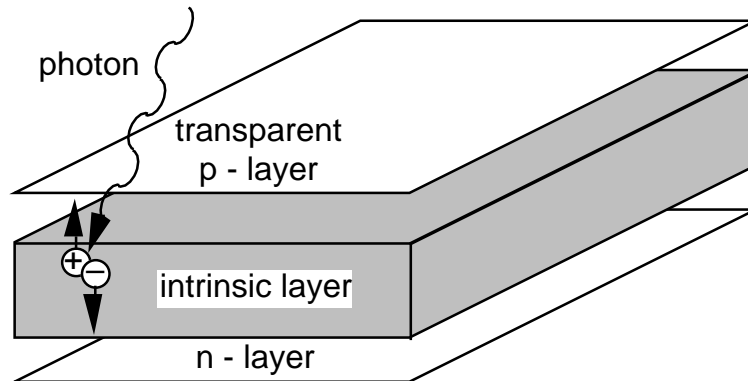


Hit crystal identified by Anger Logic

- 3 mm square crystals → 3 mm spatial resolution
- Detector block is 1 x 1 inches → 0.3 μ s in₂ dead time

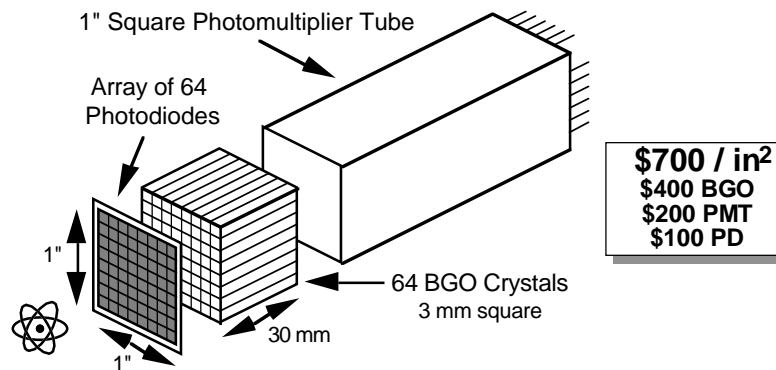
2

Silicon PIN Photodiode



- Gain = 1
- Noise = 300 electrons fwhm
- \$1 per 3x3 mm cell

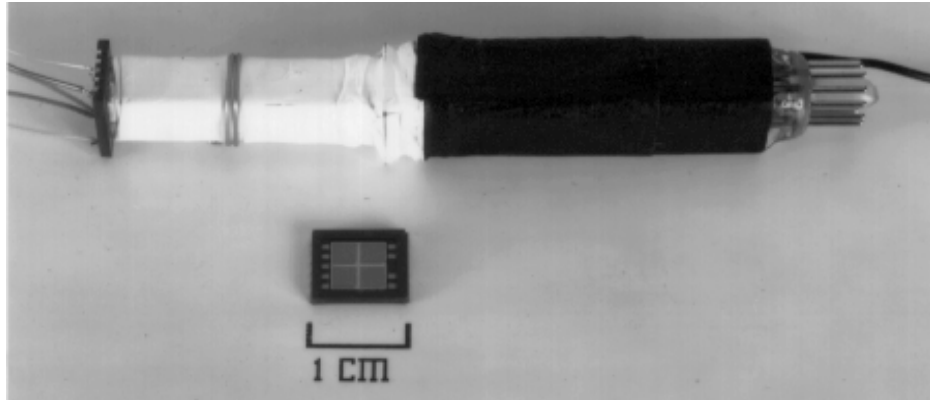
PIN Photodiode Module Design



Hit crystal identified by photodiode array

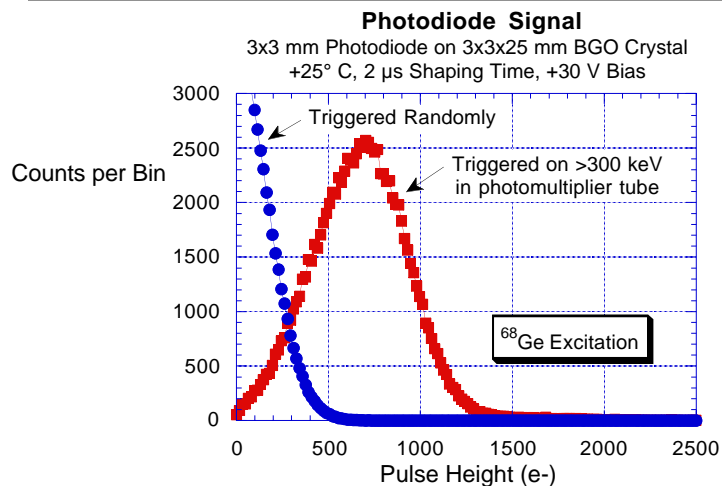
- + Economical, feasible with existing technology
- Signal to noise barely good enough - no margin for error

Prototype PIN Photodiode Module



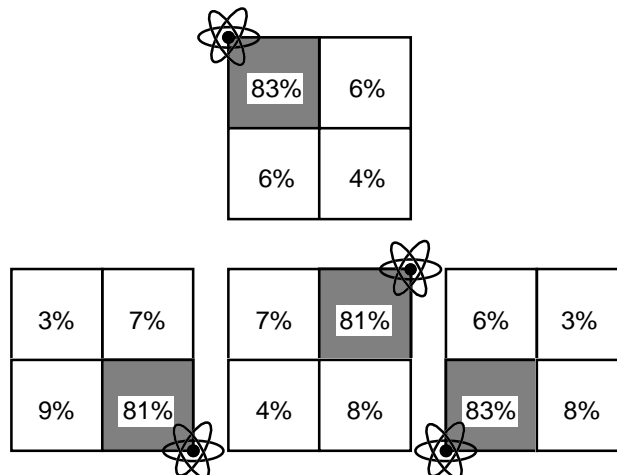
- One photomultiplier tube
- Four 3 x 3 x 30 mm BGO crystals
- Hit crystal identified with 2 x 2 photodiode array

Signal to Noise in PIN Photodiode



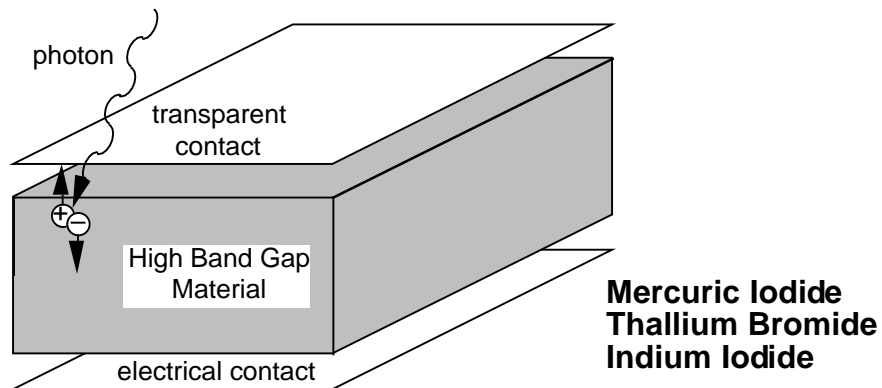
511 keV Signal is Well Separated from the Noise

Able to Identify Crystal of Interaction



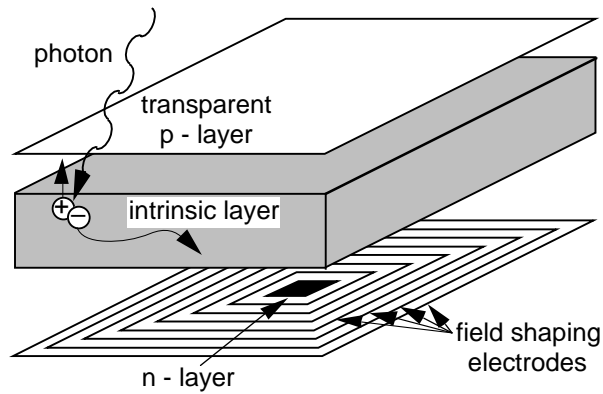
Mis-identification dominated by Compton Scatter in BGO

High Bandgap Material Photodiode



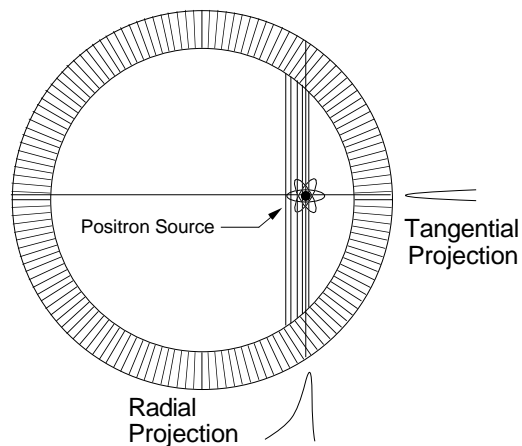
- Gain = 1
- Noise = 100 electrons fwhm
- \$2 per 3x3 mm cell?

Silicon Drift Photodiode



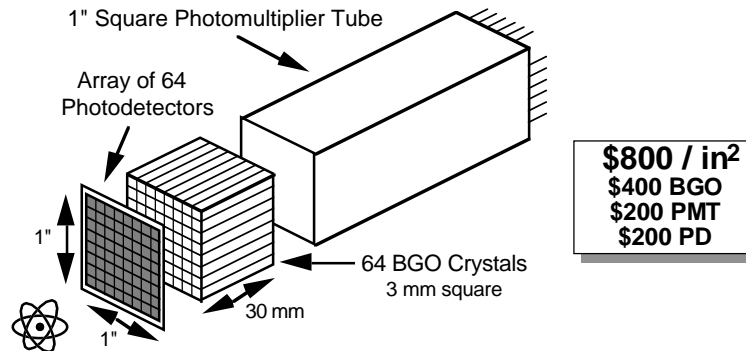
- Gain = 1
- Noise = 100 electrons fwhm
- \$2 per 3x3 mm cell?

Radial Elongation Distortion in PET



- Mis-identification from penetration into adjacent crystal
- Can eliminate if depth of interaction in crystal measured

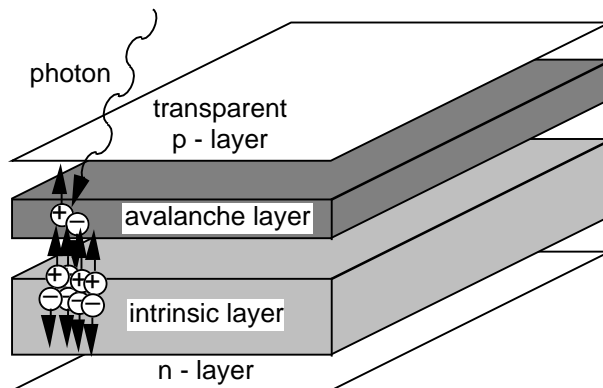
Depth of Interaction Measuring Module



Depth of interaction measured using photodetector array
(ratio of PMT signal to photodetector signal)

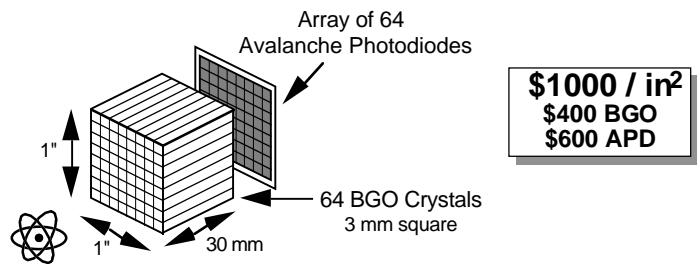
- + Good spatial resolution over *entire* field of view
- Signal to noise barely good enough - no margin for error

Avalanche Photodiode



- Gain = 200
- Noise low enough for timing
- \$10 per 3x3 mm cell?

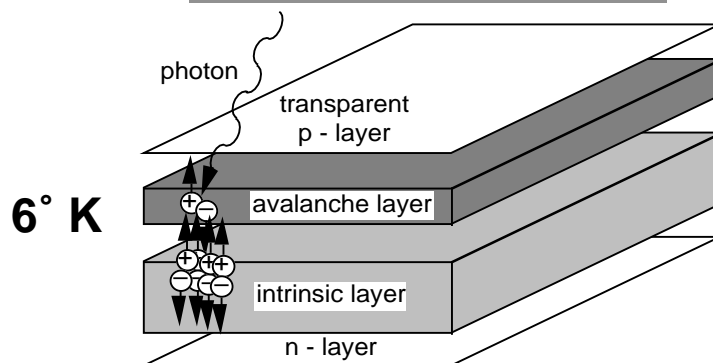
Avalanche Photodiode Module



Timing measured by avalanche photodiode array

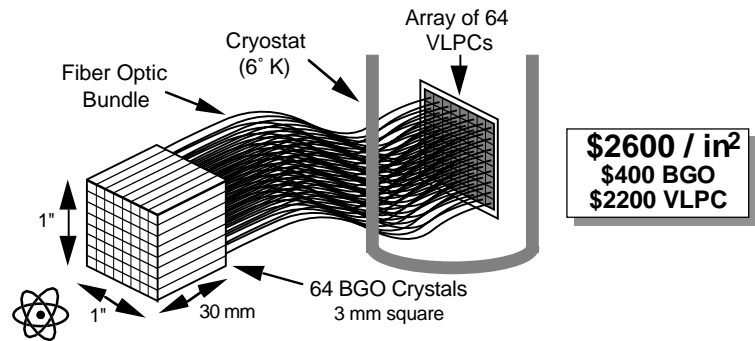
- + Electronics & packaging simpler
- Very temperature sensitive, timing barely good enough

VLPC (Visible Light Photon Counter)



- Gain = 50,000
- Noise easily low enough for timing
- \$35 per 3x3 mm cell?

VLPC Module



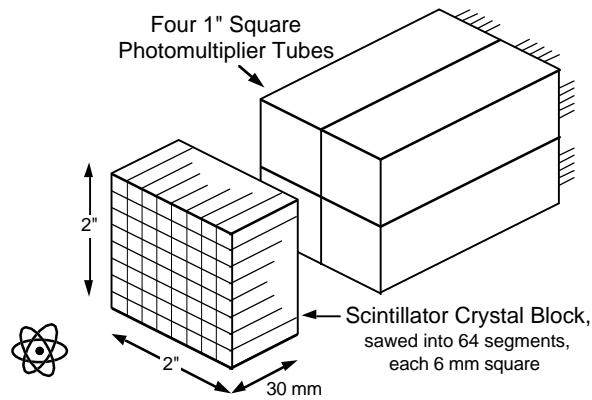
Fiber optic bundle brings light from BGO to VLPC

- + Higher gain, better timing**
- Light loss in fiber optics, VLPC operates at 6° K**

What Would You Do With a Better Scintillator?

- Shorter Decay Time**
- Higher Stopping Power**
- Higher Light Output**

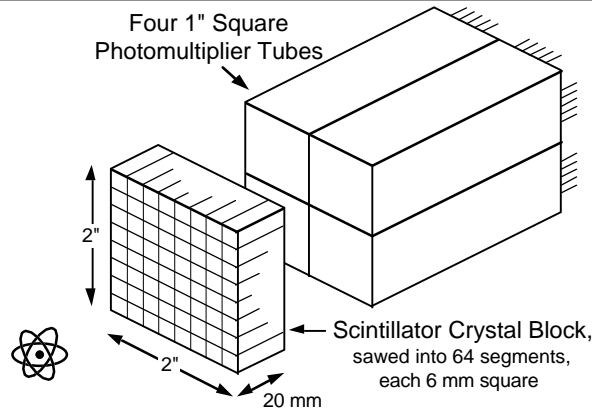
Shorter Decay Time Scintillator



Conventional configuration, but better timing resolution

- Less dead time, better image contrast (time of flight)
- Same spatial resolution (5 mm)

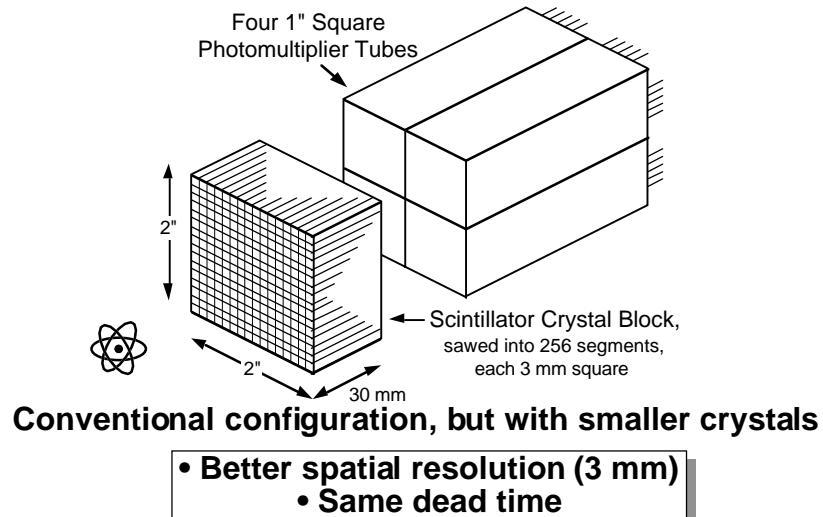
Higher Stopping Power Scintillator



Conventional configuration, but with thinner block

- Same spatial resolution (5 mm), but over larger field of view
- Same dead time, better image contrast

Higher Light Output Scintillator



Improved Scintillators ARE Possible

Example: LSO (Lutetium Orthosilicate)

- Light Output 5x More than BGO
- Decay Time 7x Faster than BGO
- Stopping Power Same as BGO
- Price 10x More than BGO

Conclusions

**Advanced Photodetectors can Improve
PET Detector:**

- Spatial Resolution
- Dead Time
- Cost

**New Scintillators can Improve All Aspects
of Detector Performance**

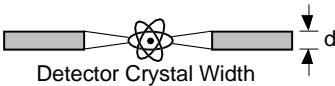

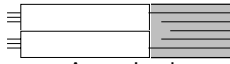

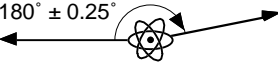

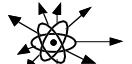

Acknowledgements

Thanks to:
Steve Derenzo, LBL

Work supported by:

- U.S. Department of Energy
Office of Energy Research, Office of Health and
Environmental Research, Medical Applications
and Biophysical Research Division, contract
No. DE-AC03-76SF00098
- National Institutes of Health
National Heart, Lung, and Blood Institute,
grant No. P01-HL25840
National Cancer Institute, grant No. R01-CA48002
National Institute of Neurological Disorders,
grant No. R01-NS29655.

Contributions to Spatial Resolution

Factor	Shape	FWHM
 <p>Detector Crystal Width</p>		$d/2$
 <p>Anger Logic</p>		0 (individual coupling) 2.2 mm (Anger logic)* *empirically determined from published data
 <p>Photon Noncollinearity</p>		1.3 mm (head) 2.1 mm (heart)
 <p>Positron Range</p>		0.5 mm (^{18}F) 4.5 mm (^{82}Rb)
Reconstruction Algorithm	multiplicative factor	1.25 (in-plane) 1.0 (axial)